Probabilistic insights into human shoulder biomechanics L. Engelhardt, W. A. Wall

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Activation

1 Introduction

Continuum mechanical models of the shoulder enable in-depth analysis of biomechanics, pathological conditions, personalized treatments, and medical device design.

Model predictions are inherently uncertain due to incomplete data, measurement errors, biological variability, and model assumptions, simplifications and errors.



2 Continuum mechanical human shoulder model

Finite-element model of the human shoulder including key physiological features



Active, passive

muscle tissue

Generalized

active strain

material model

 $\alpha, \beta, \gamma, \kappa, \omega_0$

 $\lambda_{\min}, \lambda_{opt}, P_{opt}$





Muscle fiber



Bone, cartilage, Component



Tendon



Uncertain input parameters

By propagating input uncertainty through the model, probabilistic approaches capture the full range of possible outputs, enhancing prediction robustness and reliability. Since clinical decisions are based on probabilistic data, probabilistic model predictions are indispensable for informed, evidence-based decision-making.



3 Uncertainty quantification and global sensitivity analysis

Prior Define input ranges and distributions based on domain knowledge.

Uncertainty quantification Quantify model output uncertainty due to variations in input space.

Sensitivity analysis Attribute output uncertainty to input parameters.

Gaussian process Approximate model output with trained metamodel when evaluations are costly.



4 Application examples

Uncertainty of muscle material model parameters

Uncertainty of muscular activation patterns

Uncertainty in muscular activation arises from neural noise, physiological variability, and measurement inaccuracies and incompleteness due to indirect or imprecise measurement methods.

Example: Probabilistic modeling of deltoid muscle contraction under uncertain activation

Model: Free contraction simulation of the deltoid muscle partitioned into 100 regions *i* with activations a_i .



Input X: Activation uncertainty modeled with Beta distributions with a coefficient of variation (CV) of 30%, consistent with upper bounds of intra-subject and intersession normalized EMG (%MVC) variability reported in the literature.

Output Y: Displacement magnitude of the free end node u_n as a measure for the global contraction.





large output uncertainty.



Motivation: Experimental stress-strain data on active and passive muscle tissue shows large variability. Material model parameters calibrated based on this data are thus uncertain.

Prior: Input parameter ranges determined based on 84 stress-strain curves from the literature (18 publications, eight load cases), with uniform distributions assumed.







Variability of the output deltoid contraction deformations remains lower than the assumed variability in input activations.

Subscapularis muscle contraction (quantified by the free end displacement magnitude) is dominated by the minimal fiber stretch λ_{min} . The optimal fiber stretch λ_{opt} has no influence.

5 Conclusion

- Uncertainty quantification improves result interpretability and reliability. Sensitivity analysis helps target experimental and computational efforts.
- A metamodel-based approach enables efficient global variance-based sensitivity analysis for computationally expensive models.
- As musculoskeletal models face high input uncertainty, probabilistic approaches are particularly relevant for reliable predictions, both clinically and scientifically.

